Biomechanical Differences of Lower Extremity Joints at the Frontal Plane during Sidestep Cutting in Male and Female Judo Athletes

Hyun Yun†

Department of Judo, College of Martial Arts, Yongin University, 134 Yongindaehak-ro, Cheoin-gu, Yongin-si, Gyeonggi-do 170–92, Korea
(Received January 17, 2018; Revised February 12, 2018; Accepted February 28, 2018)

Abstract: The purpose of this study was to analyze the biomechanical differences of lower extremity joints of the frontal plane during sidestep cutting in male and female Judo athletes. In the knee and hip joint, the female group showed a smaller angle than the male group at the time of IC(initial contact). But peak knee joint adduction moment of female group was greater than male group(p<.05). Therefore, female Judo athletes were more likely to injure their knees at the point where their initial foot contacted the ground than male athletes during sidestep cutting.

Keywords: Lower extremity joints, Biomechanics, Frontal plane, Judo athletes, Sidestep cutting

1. Introduction

Acute injuries of the lower extremities frequently occur in athletes performing sports activities [1]. Several previous studies on joint injuries have been reported to be relatively more frequent in female athletes than in men [2–4]. Female athletes have higher risk of contact anterior cruciate ligament injuries than male athletes, which may be due to body structure differences such as lower limb strength and Q angle [5, 6].

Judo, the official sport of the Olympic Games, has recently reduced the size of the stadium, banned lower body attacks, and imposed strict penalties on defensive players to induce more aggressive games. Judo players perform their movements quickly by attacking and defending their feet. In addition, the attack technique that supports the body weight with one foot increases the risk of injury because it increases the load on the leg joint of the foot during the defense of the opponent [7]. Induction athletes perform physical rotation exercises centering on the footsteps when attacking techniques are used to obtain the opponent’s score. At this time, the lower extremity joints are performed to a combination of adduction/abduction in the kinematic chain aspect.

Knee joint injuries to Judo players account for about 20% of total injury, and the joint injury rate of the lower limb following the arm joints that come to contact with the opponent among the injury types of Judo
players is the second [8]. In specially, differences in the motion of the lower limb joints occurring on the frontal plane during the sudden directional change affect the risk of injury to the knee joint [9]. The alignment of the lower limb joints is recognized as an important index to determine the risk of joint injuries, because sudden load occurs in the lower limb joint after foot to ground contact.

Therefore, the purpose of this study was to analyze the biomechanical differences of lower extremity joints of the frontal plane during sidestep cutting in male and female Judo athletes.

2. Methods

2.1. Subjects

The subjects of this study were 15 male (age = 22.17 ± 1.41 yrs, body weight = 75.62 ± 4.55 kg, height = 1.76 ± 0.03 m, career = 7.26 ± 1.30 yrs) and female (age = 20.92 ± 1.16 yrs, weight = 64.03 ± 6.19 kg, height = 1.64 ± 0.06 m, career = 7.80 ± 1.50 yrs) Judo athletes, who had not experienced orthopedic history and neurological history were selected. All the subjects were fully explained about the purpose of the experiment, and the experiment agreement was made.

2.2. Data collection

Height and weight were measured in all participants. Moreover, an anthropometer (SM-324) was used to measure body segment length and circumference that were required for applying the scaling method for body segment parameters. The subjects were wearing shorts and t-shirts in black spandex and participated in the experiment with their personal running shoes. Subjects were instructed to perform a directional change using a left foot at distance of 4.5m from the starting point of the pre-displayed starting point. In the direction of the subject’s motion, and the direction change performed by supporting is performed on the right side. At this time, information on the direction was recognized on the ground using a blue tape.

After sufficient stretching to prevent injury to the subjects, which could occur due to the sudden change of direction, the direction change operation was performed for 10 minutes. In order to analyze the motion of the human body in three-dimensional analysis, 35 15-mm reflective markers suitable for a plug-in-gait model were attached on the participants for 3D motion analysis during the sidestep cutting. A three-dimensional coordinate acquisition area of the cameras was created using a T-shaped wand composed of four reflective markers, and then the NLT(nonlinear transformation) to calculate the positional coordinates of the reflection markers on the human body in the 3D motion analysis. And the global coordinate system in which the forward and backward directions of the movement progression direction are defined as the Y-axis, the medial and lateral directions are defined as the X-axis, and the vertical direction is defined as the Z-axis. We defined the local coordinate system of the head, body, pelvis, femur, lower leg, foot, upper arm, forearm, and hand segment using reflection markers attached to the human body.

The visual information device LED (Light Emitting Diode, Visol, Korea) was installed at 8m ahead of the starting line to prevent the subjects from performing pre-bodily movements before the change of direction. Two electronic sensors (Photoelectric sensor, Viso, Korea) were installed at the points before redirection at intervals of 2.5 m to prevent the differences in the speed of motion in collecting the directional movement of subjects. LEDs were used to visualize the direction of the subjects. The subjects started to operate according to the first light signal of the LED. When they passed the two electronic sensors, they collected information about the
speed and transmitted the information about the redirection through the LED signal. The subjects performed a linear motion. All electronic signal equipment are A/D Sync box (VSAD-T02-32C, Visol, Korea). Biomechanical data of subjects were collected at 100 Hz using 8 Vicon cameras (T10S, Vicon, UK) and at 1000 Hz using force plate (OR6-7-1000, AMTI, Inc, Watertown, MA, USA, sampling rate).

2.3. Data analyze

In this study, to analyze the kinematic factors of the lower limb during sidestep cutting, the point where the left foot contacts the ground and the vertical repulsion force is 10N or higher is referred to as event 1 (initial contact), event 2 was max knee flexion (MKF) while the left foot was in contact with the ground, event 3 was toe off (TO).

The 3 dimensional coordinate data of the reflection markers attached to the human body were filtered by a second-order low-pass butterworth filter (6 Hz) and the data collected by the ground reaction force were filtered by a second-order butterworth filter (50 Hz).

The subjects’ data were modeled and data processed using Kwon3d XP software (Visol Inc, Korea). The cardan orientation method calculates the relative orientation angle of the distal segmental coordinate system to the proximal segmental coordinate system after setting the local coordinate system (X axis: medial/lateral direction, Y axis: anterior/posterior direction, Z axis: vertical direction). And the angle of the human joint was calculated. The kinematical data and the ground reaction force data calculated by the experiment

---

**Fig. 1. Coordinate system of lower body segment.**

**Fig. 2. Schematic diagram for computing lower extremity joints angles and moments.**
are substituted into the joint equilibrium equation which is calculated by the inverse dynamics method as biomechanical model, and the body inertia values of the subjects are calculated using the measured data joint reaction force and joint moment were calculated (fig. 2). The ankle, knee, hip joint motion was defined as the following: positive (+) and negative (−) values in the AP axis as adduction and abduction, respectively.

**2.4. Statistics**
In this study, we compared the adduction and abduction of the lower extremity joints on the frontal plane during the change of direction of the male and female Judo athletes. In order to verify the difference of analysis factors, SPSS ver. (SPSS Inc., Chicago, IL, USA) Statistical analysis was performed using independent t-test. The significance level of data processing was set to $\alpha = .05$.

### 3. Results and Discussion

(Table 1) and (Fig. 3) showed the results of the analysis of the kinematic factors in the frontal plane during the direction change of the Judo players participating in this study.

### Table 1. Biomechanical lower extremity joints angle on frontal plane between male and female

<table>
<thead>
<tr>
<th>Joint</th>
<th>Event</th>
<th>Male</th>
<th>Female</th>
<th>t-value</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Ankle</td>
<td>Initial Contact</td>
<td>−1.22</td>
<td>−0.96</td>
<td>0.590</td>
<td>.560</td>
</tr>
<tr>
<td></td>
<td>(10.15)</td>
<td>(9.65)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Max Knee Flexion</td>
<td>−7.24</td>
<td>−1.12</td>
<td>1.453</td>
<td>.158</td>
</tr>
<tr>
<td></td>
<td>(10.99)</td>
<td>(11.70)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Toe Off</td>
<td>8.18</td>
<td>6.11</td>
<td>−.746</td>
<td>.462</td>
</tr>
<tr>
<td></td>
<td>(6.77)</td>
<td>(8.14)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Knee</td>
<td>Initial Contact</td>
<td>5.94</td>
<td>0.76</td>
<td>−2.547</td>
<td>.017*</td>
</tr>
<tr>
<td></td>
<td>(6.59)</td>
<td>(3.93)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Max Knee Flexion</td>
<td>17.70</td>
<td>13.21</td>
<td>−1.739</td>
<td>.093</td>
</tr>
<tr>
<td></td>
<td>(7.24)</td>
<td>(0.06)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Toe Off</td>
<td>10.67</td>
<td>8.39</td>
<td>−.733</td>
<td>.470</td>
</tr>
<tr>
<td></td>
<td>(7.11)</td>
<td>(9.50)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Hip</td>
<td>Initial Contact</td>
<td>−10.46</td>
<td>−4.39</td>
<td>2.105</td>
<td>.045*</td>
</tr>
<tr>
<td></td>
<td>(8.59)</td>
<td>(6.76)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Max Knee Flexion</td>
<td>−10.25</td>
<td>−7.35</td>
<td>1.270</td>
<td>.215</td>
</tr>
<tr>
<td></td>
<td>(0.04)</td>
<td>(4.75)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>Toe Off</td>
<td>−5.14</td>
<td>−9.62</td>
<td>−2.026</td>
<td>.053</td>
</tr>
<tr>
<td></td>
<td>(5.89)</td>
<td>(6.00)</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Note. *$p<.05$
There was no statistically significant difference between the male and female groups at the IC (t=0.590, p=.560), MKF (t=1.453, p=.158), and TO (t=-0.746, p=.462) in the ankle joint. In the knee joint, the female group showed a smaller angle than the male group at the time of IC (t=-2.547, p=.017). MKF (t=-1.739, p=.093) and TO (t=-0.733, p=.470) showed no statistical difference between the two groups.

In the hip joint, the female group showed a smaller angle than the male group at the time of IC (t=2.105, p=.045). MKF (t=1.270, p=.215) and TO (t=-2.026, p=.053) showed no statistical difference between the two groups.

(Fig. 4) shows the results of analysis of the peak add/abduction moments of the left lower extremity joints of the male and female group in the sidestep cutting. There was no statistically significant difference between the male and female groups in the factors of peak add/abduction moment of the ankle (t=0.290, p=.774) and hip (t=1.042, p=.307) joints in the turning direction. Only the peak add/abduction moment of the knee (t=2.807, p=.009) joint showed statistical differences between the two groups.
The level of the repulsive force of the ground that occurs during the body deceleration exercise increases the risk of non-contact injury of the knee joint [10]. During the body decelerating movement, a large load is generated in the knee joint with the contact of the foot and the ground, and the anterior movement of the femur due to the movement of the ankle and the knee joint can be improved. And it is reported that this increases the risk of injury to anterior cruciate ligament [6, 11, 12].

It has been reported that the adduction moment generated by the add/abduction of the supporting foot and the increase of the extension moment due to the extensor contraction of the quadriceps muscle increase the compressive force and shear force of the knee joint [13, 14].

In this study, the female group was smaller than the male group in the add/abduction angle of the supporting foot of the knee and hip joint at the initial contact with the ground. Movement of the knee joint at the time of changing direction of the body movement affects the maximum add/abduction moment of the knee joint [15, 16]. This increase in the moment of the knee joint increases the compressive force and shear force of the knee joint with the increase of the extension moment due to the stretch contraction of the quadriceps muscle [4, 17]. The result of this study showed that the knee joint adduction moment of female Judo group in induction was higher than that of male Judo group [16, 18].

4. Conclusions

The purpose of this study was to analyze the biomechanical differences of lower extremity joints of the frontal plane during sidestep cutting in male and female Judo athletes. In female group, the angle of knee and hip joint was smaller than that of male Judo player at the initial contact point. The peak adduction/abduction moment of the knee joints of female Judo players group were higher than those of male during the sidestep cutting performance. Therefore, we found that the risk of injuries to knee joints in female Judo athletes was relatively higher than that of male Judo athletes during a sudden exercise in the side direction.

Acknowledgements

This paper was supported by Yongin University research funding in 2016.

References