

Feasibility Study of Patient Specific Quality Assurance Using Transit Dosimetry Based on Measurement with an Electronic Portal Imaging Device

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Myonggeun Yoon (radioyoon@korea.ac.kr) Tel: 82-2-3290-5651 Fax: 82-2-921-6434 This study was designed to measure transit dose with an electronic portal imaging device (EPID) in eight patients treated with intensity modulated radiotherapy (IMRT), and to verify the accuracy of dose delivery to patients. The calculated dose map of the treatment planning system (TPS) was compared with the EPID based dose measured on the same plane with a gamma index method. The plan for each patient was verified prior to treatment with a diode array (MapCHECK) and portal dose image prediction (PDIP). To simulate possible patient positioning errors during treatment, outcomes were evaluated after an anthropomorphic phantom was displaced 5 and 10 mm in various directions. Based on 3%/3 mm criteria, the mean±SD passing rates of MapCHECK, PDIP (pre-treatment QA) for 47 IMRT were 99.8±0.1%, 99.0±0.7%, and, respectively. Besides, passing rates using transit dosimetry was 90.0±1.5% for the same condition. Setup errors of 5 and 10 mm reduced the mean passing rates by 1.3% and 3.0% (inferior to superior), 2.2% and 4.3% (superior to inferior), 5.9% and 10.9% (left to right), and 8.9% and 16.3% (right to left), respectively. These findings suggest that the transit dose-based IMRT verification method using EPID, in which the transit dose from patients is compared with the dose map calculated from the TPS, may be useful in verifying various errors including setup and/or patient positioning error, inhomogeneity and target motions.

Keywords: Linear accelerator, Transit dose, EPID, Gamma index

Introduction

Novel radiotherapy methods, including intensity modulated radiotherapy (IMRT), volumetric modulated arc therapy (VMAT) and heavy ion therapy, all of which are more advanced modalities than conventional 3D conformal radiation therapy, have recently been implemented clinically. These methods reduce exposure to radiation of a patient's normal tissues and surrounding organs while increasing radiation dose to tumors.¹⁻³⁾ For treatment purposes, the radiation dose calculated from a treatment planning system (TPS) should be accurate. In addition, care should be taken during radiation delivery because IMRT consists of a complex delivery system, with treatment beams having large monitor units (MUs), which may cause critical damage if errors occur during treatment. Therefore, a quality assurance (QA) program is essential to verify the difference between dose distribution calculated from TPS and the actual dose distribution during the complex IMRT treatment procedure, which involves many

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small fields with varying dose intensities.⁴⁻⁶⁾

Conventional QA of IMRT is performed prior to treatment, verifying the actual dose with an ion chamber using a homogeneous phantom or evaluating dose distribution on a 2D plane. Methods using homogeneous phantoms can only verify the delivery of an intensity modulated beam (IMB) and the accuracy of dose distribution in homogeneous matter. Because conventional IMRT OA does not consider the heterogeneity in real patients, such as air cavities and bony structures,^{7,8)} it cannot assure the accuracy of the actual dose distribution to patients. Nevertheless, the estimated value from TPS and the measured value from QA are consistent. Portal dose image prediction (PDIP) using an electronic portal imaging device (EPID) was recently implemented clinically for pre-treatment QA.^{9,10)} This QA method can also verify the difference between the dose distribution calculated from TPS and the dose distribution actually delivered, thus providing accurate IMB delivery. Furthermore, conventional pre-treatment IMRT QA methods do not provide information on actual beam delivery during treatment, since various errors, such as patient movement during treatment, cannot be determined. Therefore, current QA methods may be considered unacceptable in verifying the actual dose delivered to patients.^{11,12)}

These drawbacks of current QA methods may be eliminated by transit dosimetry, measured using 2D detectors in the treatment room. To date, various studies have assessed transit dosimetry at the position of the EPID behind a patient.¹³⁻¹⁵⁾ Comparisons of dose distributions by transit dosimetry in homogeneous solid water phantoms and heterogeneous anthropomorphic phantoms showed that substantial errors were caused by heterogeneous media.^{16,17)} To verify the effectiveness of the suggested method, it is necessary to test it in actual patients. This study therefore measured transit doses passing through real patients using EPID during treatment and compared it with doses calculated from TPS. The experimental results suggested that this transit dosimetry based IMRT verification method may provide proper QA of actual doses delivered to patients by detecting random and systematic errors during treatment.

Materials and Methods

Eight patients undergoing IMRT were selected (Table 1). During treatment, the transit dose of each treatment field was measured using an aS1000 EPID attached to a Varian Clinac iX linear accelerator (Varian Medical Systems, Palo Alto, CA) (Fig. 1). According to the vendor's guidelines, EPID was calibrated for transit dose analysis with a dark field, a flood field and a diagonal profile correction at d_{max} in water for a 40×40 cm² open field. The EPID response was scaled such that 1 Calibrated Unit (CU) corresponded to 100 MU delivered by a 10×10 cm² open field at 100 cm source-to-detector distance (SDD). The estimated nonuniform back-scatter pattern was corrected to remove any non-uniform backscattering pattern during the calibration process. The absolute dose of the transit beam was first measured with EPID in calibrated units (CU) and converted to the absorbed dose using the calibration curve. The EPID system used in this study was an amorphous silicon flat panel imager type, with an active imaging area measuring 30×40 cm², and a field of view at the isocenter

| Patient number | Treatment Site | Photon Energy | PTV (ml) | Number of fields | IMRT delivery technique | | | | |
|----------------|-----------------|---------------|----------|------------------|-------------------------|--|--|--|--|
| 1 | Maxillary sinus | 6 MV | 130.3 | 7 | DMLC | | | | |
| 2 | Cervix | 6 MV | 171.4 | 5 | DMLC | | | | |
| 3 | Prostate | 6 MV | 101.6 | 7 | DMLC | | | | |
| 4 | Eye | 6 MV | 86.4 | 5 | DMLC | | | | |
| 5 | Lung | 6 MV | 154.5 | 5 | DMLC | | | | |
| 6 | Brain | 6 MV | 235.3 | 5 | DMLC | | | | |
| 7 | Oropharynx | 6 MV | 228.8 | 7 | DMLC | | | | |
| 8 | Brain | 6 MV | 122 | 6 | DMLC | | | | |

 Table 1. Demographic and radiologic characteristics of the eight patients analyzed in this study.

DMLC: Dynamic Multileaf collimator.



Fig. 1. EPID measurements of transit doses during treatment at the posterior surfaces of Patients (a) 1 (maxillary sinus) and (b) 3 (prostate).

Table 2. Pre-treatment passing rates (%) of results measured with MapCHECK (M) and PDIP (P) based on the gamma index for the eight included patients.

| Patient | Field number | | | | | | | | |
|---------|-----------------|-------|-------|-------|-------|-------|-------|-------|-------|
| No. | Dosimetric tool | 1 | 2 | 3 | 4 | 5 | 6 | 7 | Mean |
| 1 | М | 100.0 | 99.8 | 100.0 | 100.0 | 99.7 | 97.7 | 100.0 | 99.6 |
| | Р | 99.5 | 99.3 | 96.0 | 99.4 | 99.6 | 98.6 | 95.7 | 98.3 |
| 2 | Μ | 99.1 | 100.0 | 100.0 | 99.6 | 100.0 | | | 99.7 |
| | Р | 99.9 | 96.9 | 99.7 | 99.9 | 99.9 | | | 99.3 |
| 3 | М | 100.0 | 99.8 | 100.0 | 98.9 | 100.0 | 99.8 | 100.0 | 99.8 |
| | Р | 99.9 | 99.8 | 100.0 | 97.0 | 98.9 | 97.9 | 99.9 | 99.1 |
| 4 | Μ | 100.0 | 100.0 | 100.0 | 100.0 | 100.0 | | | 100.0 |
| | Р | 99.9 | 98.7 | 100.0 | 98.4 | 99.9 | | | 99.4 |
| 5 | М | 99.8 | 100.0 | 99.1 | 100.0 | 100.0 | | | 99.8 |
| | Р | 99.7 | 100.0 | 98.5 | 99.9 | 99.9 | | | 99.6 |
| 6 | Μ | 100.0 | 100.0 | 100.0 | 100.0 | 100.0 | | | 100.0 |
| | Р | 99.9 | 99.9 | 100.0 | 99.9 | 99.9 | | | 99.9 |
| 7 | М | 98.9 | 100.0 | 99.8 | 100.0 | 99.4 | 100.0 | 99.8 | 99.7 |
| | Р | 97.7 | 100.0 | 99.0 | 99.4 | 98.8 | 98.9 | 97.4 | 98.7 |
| 8 | Μ | 99.1 | 98.9 | 100.0 | 100.0 | 100.0 | 99.4 | | 99.6 |
| | Р | 96.4 | 95.8 | 95.2 | 99.8 | 98.8 | 98.7 | | 97.5 |

from 25×33 cm² to 16×22 cm². This EPID has a $1,024 \times 768$ pixel matrix, 0.392 mm of pixel pitch, and an energy range of 4–25 MV. The transit doses were measured using 6 MV beams at a source-to-detector distance (SDD) of 150 cm.

Planned dose distributions were calculated with the Eclipse treatment planning system Ver 8.9. (Varian Medical Systems, Salt Lake City, UT, USA), using an anisotropic analytical algorithm (AAA). Conventional pre-treatment QAs were determined using MapCHECK (Sun Nuclear, Melbourne, FL) and Portal Dose Image Prediction (PDIP). MapCHECK has 1527 diode detectors with 7.07 mm uniform spacing across an area of 32×26 cm². Each detector

has active area of $0.8 \times 0.8 \text{ cm}^2$, a thickness of 2.0 g/cm² and a thickness of backscatter of 2.75 g/cm². To simulate possible setup error situation during treatment, transit doses were measured after displacing the heterogeneous anthropomorphic phantom from its original position by 5 and 10 mm in the superior to inferior (SI), inferior to superior (IS), right to left (RL), and left to right (LR) directions.

The gamma evaluation method was used to compare doses calculated from TPS with measured doses, using 3% dose difference (DD) and 3 mm distance-to-agreement (DTA) criteria.¹⁸⁾

Results

Table 2 shows the results of pre-treatment QA for 47 IMRT fields acquired from eight patients using MapCHECK and PDIP methods. Values calculated from the TPS were well matched with the measured value from the two QA methods. The mean passing rates of QA results based on MapCHECK and PDIP were $99.8\pm0.1\%$ and $99.0\pm0.7\%$, respectively, showing that the doses measured on the homogeneous phantom (i.e., MapCHECK) and on the fluence map with EPID were well matched with doses calculated from TPS.

Fig. 2A and B show the calculated and measured dose maps, respectively, of transit doses passing through field 3 of patient 1 in Table 2. For this field, the passing rate was 90.5%, indicating that the transit dose map measured with the EPID was relatively well matched with the dose distribution calculated by the TPS. Table 3 shows the

detailed passing rates for the 47 IMRT fields. Analysis of the calculated transit doses using the actual patients, however, showed more regions with gamma index (GI) more than 1, indicating an increased percentage of failure. Detailed gamma analysis of transit dosimetry with actual patients showed that the passing rates are generally decreased, to a mean±SD of 90.0±1.5% (Table 3). Passing rates were therefore about 9-10% lower using transit dosimetry than conventional pre-treatment IMRT as a QA tool. To determine whether transit dosimetry could detect random errors during treatment, radiation was deliberately delivered with a setup error and the changes in the transit dose distribution were evaluated.

Discussion

This study compared the transit doses of 47 IMRT fields measured with an EPID with the doses calculated from



Fig. 2. Transit doses in field 3 from Patient 1 (a) calculated from TPS and (b) measured using EPID.

Table 3. Passing rates of results measured using transit dosimetry based on the gamma index values for the eight patients.

| Patient | Field number | | | | | | | | |
|---------|--------------|------|------|------|------|------|------|------|------|
| No. | t | 1 | 2 | 3 | 4 | 5 | 6 | 7 | Mean |
| 1 | 3%/3 mm | 90.0 | 83.1 | 90.5 | 92.4 | 93.3 | 88.0 | 89.6 | 89.6 |
| 2 | 3%/3 mm | 95.1 | 86.7 | 94.9 | 86.5 | 85.4 | - | - | 89.7 |
| 3 | 3%/3 mm | 96.5 | 96.4 | 86.8 | 79.4 | 84.9 | 91.6 | 95.3 | 90.1 |
| 4 | 3%/3 mm | 94.9 | 95.3 | 92.4 | 95.9 | 87.3 | - | - | 93.2 |
| 5 | 3%/3 mm | 89.2 | 87.9 | 82.7 | 94.0 | 86.5 | - | - | 88.1 |
| 6 | 3%/3 mm | 94.9 | 93.4 | 81.4 | 92.9 | 94.1 | - | - | 91.3 |
| 7 | 3%/3 mm | 89.6 | 92.9 | 90.0 | 91.8 | 87.2 | 87.6 | 86.4 | 89.4 |
| 8 | 3%/3 mm | 96.2 | 88.0 | 89.7 | 86.4 | 86.9 | 82.5 | - | 88.3 |

TPS. Although the measured and calculated transit doses were relatively well matched, the passing rates in some treatment fields were lower than in others. For example, the mean passing rate of five IMRT fields in patient 5 was 88.1±3.7%, much lower than the mean passing rate of 93.2±3.2% for five IMRT fields in patient 4. Reduced passing rates observed in actual patients were likely due to the inaccuracy of TPS calculations of inhomogeneity. That is, although the calculation algorithm of the TPS worked well for homogeneous phantoms, it was less accurate for inhomogeneous materials such as the human body. Fig. 3 presents an example of a GI map, showing the high passing rates with MapCHECK and PDIP but a relatively lower passing rate with EPID data of an actual patient.



Fig. 3. Dose maps calculated in field 3 of Patient 2 by (a) MapCHECK and (b) PDIP and measured by transit dosimetry at (c) 3%/3 mm and (d) 5%/3 mm.

Table 4. Decreases in passing rates for phantom movement compared with the original passing rate without movement.

| Patient number | IS | | SI | | LR | | RL | |
|-------------------|------|-------|------|-------|------|-------|------|-------|
| | 5 mm | 10 mm |
| 1 | 1.8 | 4.1 | 3.0 | 6.5 | 5.3 | 9.7 | 7.6 | 13.6 |
| 2 | 0.9 | 3.8 | 2.3 | 3.3 | 6.3 | 12.3 | 10.0 | 19.0 |
| 3 | 1.8 | 2.8 | 2.5 | 4.7 | 7.0 | 12.7 | 9.9 | 18.4 |
| 4 | 1.5 | 2.7 | 1.7 | 4.2 | 5.2 | 9.4 | 8.0 | 14.4 |
| 5 | 0.7 | 1.7 | 1.3 | 2.6 | 5.7 | 10.5 | 9.0 | 16.0 |
| Mean | 1.3 | 3.0 | 2.2 | 4.3 | 5.9 | 10.9 | 8.9 | 16.3 |
| SD | 0.5 | 0.9 | 0.6 | 1.3 | 0.7 | 1.3 | 1.0 | 2.1 |

In the experiment of setup error, the measured results were compared with the original passing rate using GI analysis (Table 4). Shifts in the phantom by 5 and 10 mm in the IS, SI, LR, and SI directions reduced the mean GI average passing rates by 1.3% and 3.0%, 2.2% and 4.3%, 5.9% and 10.9%, and 8.9% and 16.3%, respectively.

These findings indicate that transit dosimetry using change in transit dose distribution may be useful in verifying setup and/or patient positioning errors caused by patient movements and resulting in inter- or intrafractional target motions.

Conclusion

This study used EPID to evaluate transit dosimetry based IMRT QA. While the IMRT QA results measured with MapCHECK and PDIP agreed well with the calculated dose, the failure rate was noticeably higher for actual patients. These findings suggest that conventional IMRT QA using homogeneity phantom may not be sufficiently accurate if inhomogeneities are present in the beam path. Our experimental results indicate that transit dosimetry may provide more accurate QA of IMRT plans than conventional IMRT QA and may also be used as a monitoring tool to verify dose delivery during treatment.

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Conflicts of Interest

The authors have nothing to disclose.

Availability of Data and Materials

All relevant data are within the paper and its Supporting Information files.

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